Optical marking of alcohol induced hemoglobin modification

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Abstract

The goal of this study is to verify whether the conformational modifications in hemoglobin molecules induced by ethanol consumption can be detected by means of optical spectroscopy. Two approaches based on comparative spectral investigations of hemoglobin samples extracted from alcohol and non-alcohol treated rats have been used, namely: we studied 1) hemoglobin oxygenation kinetics and 2) affinity of hemoglobin molecules to Cibacron Blue dye. We found that after four months of alcohol consumption the fractional weight of oxyhemoglobin has decreased whereas methemoglobin amount increased. Further alcohol consumption is accompanied by the recovery of the normal level of hemoglobin derivatives. This is in agreement with well known phenomenon of adaptation to chronic ethanol exposure. Analysis of the spectra for hemoglobin water solution doped by Cibacron Blue dye shows that dye affinity of hemoglobin is better in alcohol treated rats compared to untreated controls. Results of both approaches confirm that structural pathologies in blood protein molecules induced by ethanol and its metabolites can be detected using optical spectroscopy.

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1.Introduction

Classification of alcoholism as a mental disease, including its genetic etiology, is a dominating conception for this pathology in current medical literature [1]. Such an approach is quite perspective because it implies that the predisposition to this pathology can be detected, its prophylaxis and early diagnosis suppose to be possible and finally that as a disease it can be treated. Understanding of the origin of clinical characteristics of

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alcoholism as well as other mental diseases is complicated by the inaccessibility of the cerebrum as the main investigation object. One of the main directions of the development of non-invasive techniques for diagnosis of mental diseases traditionally is the examination of biological liquids (blood, urine, liquor, etc.) [2]. There are numerous biochemical and biophysical characterization techniques for the detection of pathological features accompanying a disease, which can be searched in the properties of biological liquids or their components. In many cases these features are related to the presence of a substance, so-called *biomarker*, unambiguously pointing to the disease. The detection of biomarkers is based on their specific biochemical properties: characteristic chemical reactions, special response to external actions [3,4] etc. and, thus, in a wider sense a biomarker can be interpreted as a specific property of the investigated biological substance, unambiguously indicating the pathology. Features accompanying a disease and consisting in deviations in chemical composition and/or concentration of the biological liquids, and which in limiting cases reduce to the absence/presence of some composition components (substances or bodies) or in the disturbances of their biochemical activity can be classified as *biochemical markers*. However, it is clear that according to the definition given above the biochemical markers do not cover all the features, which can be classified as markers of a disease, because there are those that, strictly speaking, do not imply changes in chemical composition, but consist in the modifications of the structural organization of the complex components of biological liquids, such as conformational modifications of biological molecules (in particular in proteins), in pathological changes in the cell membranes, including possible phase transitions, modifications of their surface curvature, changes in their permeability etc. (review on physical aspects of cell membrane structure can be found in [5]); we call such features *structural markers*.

Optical investigations of isotropic solutions of biologic materials are capable to bring structural information for biologic macromolecules. In the sequel we call *optical markers* those biochemical and structural markers that are detected with optical techniques. The importance of the detection of optical markers and understanding their origin on the molecular level in relation to the clinical picture of a disease is hard to overestimate accounting their non-invasive character especially for early diagnostics, including the diagnostics of latent forms of a disease.

In this paper we focus on spectral investigations of isotropic water solutions of hemoglobin samples extracted from rats and their posterity, protractedly intoxicated by ethanol, and compare these results to those obtained from the rats free of ethanol intoxication. The aim of this study is the detection of optical markers in hemoglobin molecules induced by ethanol consumption.

2.Spectra of hemoglobin from rats subjected to chronic ethanol intoxication 2.1.Basic ideas

The investigation on the biochemical markers of mental diseases and particularly of alcoholism is represented in the literature by numerous publications (see [6-12]. For example, it was found that the weight of protein fractions of blood serum at the ethanol

intoxication is changed in comparison with that in the absence of alcohol intoxication. Depression of hemocoagulation [10] the increase of circulated blood volume [11], the decrease in the number of erythrocytes, the increase of the hemoglobin amount and the increase of the amount of fetal haemoglobin [12] have also been identified as characteristic features accompanying alcoholism. They can be classified as biochemical markers of alcoholism. Biochemical markers of alcoholism are divided into two groups: markers of the pathological process (state markers) [13,14] and markers of liability to the disease (trait markers) [15]. Lack of activity of ferment Alcohol dehydrogenases is an example of a trait marker. Lack of this ferment in the organism leads to the enhancement of acetaldehyde concentration in the organism that is accompanied by unpleasant feelings, which play a repelling role and form distaste to the excessive alcohol drinking or even induces total abstinence.

Concerning the structural markers the information in the literature is rather sporadic [16]. The scarcity of investigations in this direction can be mainly related to difficulties in the sample preparation. Indeed, most of characterization techniques, that provide structural information, request uniform anisotropic samples, in particular of high optical quality for optical characterization. There are very few techniques for preparation of anisotropic biological samples (see for example [17-21]). In some cases structural information can be obtained using powdered, unaligned or liquid isotropic samples. There are several findings in current literature, which can serve as basic ideas behind the optical detection of biological markers of alcoholism. One of the pathologies caused by alcoholism is the anemia [22,23] consisting in deficiency of red blood cells and/or hemoglobin and resulting in a reduced ability of blood to transfer oxygen to the tissues (consequently causing tissue hypoxia, in particular pericentral hepatic hypoxia [24]). From molecular point of view this pathology is related to the presence of acetaldehydes in biological liquids. Acetaldehydes are products of ethanol oxygenation reactions. The acetaldehyde can interact with proteins and enzymes and induces their modification. Modifications of non-enzyme proteins consist in conformational changes of their molecular structure and, as a result lead to a disturbance of their biological functions. In particular, it is known that acetaldehyde can create complexes with the blood serum albumin; modifies the iron transferring-mediator and hemoglobin-oxygen-transportation proteins [22]. In addition acetaldehyde can have indirect effects, namely, stimulating the peroxide lipid oxidation. Referring to peroxide lipid oxidation, we have in mind the increased level of active metabolites, such as mulonic dialdehyde, as well as the other aldehydes and cetons that manifest cytotoxic influence and are actively modifying agents [7]. These processes induce hyper-production of oxygen in the mitochondria and creation of strong oxidizer, the super oxide anion (O_2^-) . The latter participates in oxygenation of fatty acids, the components of phospholipids. Thus, entering into the organism, ethanol causes, directly or indirectly, a wealth of secondary metabolites, which induce a disturbance of cytoskeletons of cells, membranes of cell organelles, modify biologically important macromolecules and change their functions [8]. Chemical and structural modifications of blood proteins can be detected via modifications in their optical spectra with respect to the corresponding spectra for proteins in the absence of pathology.

Binding of ligands is a property of protein molecules that definitely depends on their conformational state. If a ligand is a light absorbing material (a dye), then affinity of the protein molecules to dye molecules can be characterized studying absorption spectra of the protein solutions doped with dye. Therefore, adding dyes to hemoglobin samples one can visualize structural differences in protein molecules extracted either from alcohol intoxicated $AI_{i,j}$ or non-intoxicated AF groups of rats studying absorption spectra.

To detect conformation modifications of proteins one uses ability of some dye molecules to bound protein molecules. The conformation modifications of protein molecules change their affinity to the dye molecules, i.e. the number of the dye molecules attached to the protein molecules depends on the conformation state of the protein molecule. The idea behind is that the spectra of the proteins with dye molecules attached to them differ from those, which are obtained when the dye molecules do not bind the protein molecules. Comparing spectra for dye doped water solutions of hemoglobin extracted from blood taken from animals of $AI_{i,j}$ and AF groups we expect to detect the

difference in the conformation states of hemoglobin for these groups.

2.2.Experimental

Females of white rats selected with an average weight of 250g have been placed into single cages and separated in two groups, namely: Alcohol Intoxicated group ($AI_{i,j}$, where *i* denotes the duration of alcohol intoxication in months and j = 0,1,2,3 indicates the generation with j = 0 corresponding to the parents or to the animals whose posterity has been not investigated) with free access to 15% water solution of ethanol instead of water and Alcohol Free (*AF*) group without ethanol intoxication (consumption of water without ethanol).

The rats were copulated at the age of four months after one month of ethanol feeding. Newly born animals separated from their parents have been also fed with ethanol such that their daily ethanol dose was about 4.0-6.0 g/kg. Females have continued to intake ethanol during gestation. Amount of consumed liquid and the weight of animals were daily controlled. A parameter a_m calculated as the ratio of the mass of consumed ethanol over the mass of a given animal and characterizing alcohol motivation has been determined for each animal. If $a_m > 7$ g/kg we conclude that there is alcohol motivation. In 10 days rats with evident alcohol motivation were selected for further forcible alcohol intoxication. The blood sampling from the tail vein for further investigation was performed after *i* months of 15% ethanol consumption. For comparison the blood from *AF* group of animals without ethanol intoxication was similarly studied. All the rats, including those of the control group were accommodated at the same conditions (feeding, lightening, etc.).

To prepare hemolysate we have used heparin as anticoagulant. Plasma was separated centrifuging whole heparinizated blood. Hemolysis of red blood cells was performed with 30mM K-, Na-phosphate buffer (pH 7.36). Hemoglobin was extracted from blood following the technique described in (see e.g. [12] for details). The separated hemoglobin was transformed into cyanmethemoglobin (CNMetHb) and methemoglobin (MetHb); their concentrations were determined measuring their light absorption.

To study the conformational modifications in hemoglobin (Hb) following the approach described in reference [12] we used dye: Cibacron Blue (8mg of Cibacron Blue dissolved in 100ml of 0.1M acetate buffer with pH=4.8). Optical spectra were measured using spectrometer Specord M-40 in the spectral range 450-750 nm.

Stability of erythrocyte membranes was studied with the method of acid erythrograms. Erythrocytes were separated from the whole blood plasma by the centrifugation (2000 rpm) for five minutes. The erythrocyte suspension was treated three times with 0.9% solution of NaCl. Hemolysis was performed at 0.004M HCl. Erythrograms were plotted using the results of measurements obtained with photoelectrical calorimeter KFK-3.

2.3. Absorption spectra of hemoglobin

<u>Oxy- vs. deoxy-hemoglobine from $AI_{1,0}$ and AF groups.</u> Depending on the method of preparation the extracted hemoglobin can be in chemically different forms. Light absorbing spectra of deoxygenated (deoxy-Hb, other names: unsaturated or reduced) hemoglobin and oxyhemoglobin (oxy-Hb) differ and this allows one to estimate their respective amount in the sample. Fig. 1 shows absorption spectra for $AI_{1,0}$ and AF groups, namely dispersion of the molar extinction coefficient *e* of hemoglobin calculated as:

$$e = A \frac{M}{cd},\tag{1}$$

where $A = -\log_{10} (I/I_0)$ is the light absorbance of the sample with the light intensities entering and exiting from the sample here denoted as I_0 and I, respectively; M = 64500 g/mole is the molar mass of hemoglobin; c in units [g/l] is the concentration of hemoglobin and d is the distance of light passed in the sample. According to the literature data [25] presence of a broad absorption band with the maximum at $\lambda = 556$ nm is a characteristic feature of the deoxy-form of hemoglobin. Oxy-hemoglobin displays two characteristic absorption maximums at $\lambda_1 = 542$ nm, $\lambda_2 = 576$ nm and minimum at $\lambda = 560$ nm. Light absorption coefficient measured at $\lambda = 560$ nm can be used for monitoring of the deoxygenation kinetics. Qualitatively spectra are similar for all the studied samples of $AI_{i,j}$ and AF groups. However they differ quantitatively though being prepared following exactly the same procedure described above. The two plots in Fig. 1 have two isobestic points, namely at 590 and 805 nm, confirming that concentrations of hemoglobin in both AI and AF samples are equal. The absorption value at the wavelength $\lambda = 560$ nm is higher for AI_{*i*,*j*} groups than it is for the AF group. This latter suggests that the venous blood of the ethanol intoxicated rats appears to be enriched by deoxy-Hb form in comparison with the group AF free from ethanol intoxication. We investigated this suggestion comparing kinetics of hemoglobin deoxygenation for alcohol and non-alcohol treated rats.



Fig. 1. Absorption spectra of hemoglobin from alcohol treated ($AI_{1,0}$ group: solid curve) and non-treated (AF group: open circles) white rats.

Deoxygenation kinetics for AI_{1.0} and AF groups. Deoxygenation kinetics can be studied performing direct blood gas analysis [3,26] or spectroscopically measuring the light absorption at a certain wavelength (see for example [27]. Deoxygenation of hemoglobin is induced following special procedure based on reduced pressure using modified saturator [28]. Below we demonstrate that the kinetics of deoxygenation is different for the $AI_{i,i}$ and AF groups. We related this difference to the action of ethanol on the structure of the hemoglobin molecule. The time dependencies of Hb deoxygenation rate have been studied by means of spectroscopic absorption technique at the wavelength 560nm. In due course of the deoxygenation procedure the light absorption at $\lambda = 560$ nm increases and its relative increase is evident in Fig. 2, where the ratio $I(t)/I_0$ of the adsorption at a given moment t, counted from the beginning of the deoxygenation procedure, over that for t=0 is shown. It is seen that the rate of deoxygenation is higher for hemoglobin extracted from $AI_{1,0}$ group than it is for AF group. In Fig. 3 we plotted the rates of deoxigenation calculated as time derivatives of the dependencies $I_t(t)/I_0$ in due course of deoxigenation process. For the $AI_{1,0}$ group the rate of deoxygenation reached its maximal value at $t = 4 \min$, while for the AF group the maximal rate of deoxygenation is at 5.5 minute.



Fig. 2. Kinetics of deoxygenation for hemolysate extracted from rats of $A_{1,0}$ (triangles) and AF control groups (circles).



Fig. 3. Time dependencies of deoxy– genation velocity (plotted using data shown in Fig.2) for hemolysate extracted from alcohol treated rats, group $AI_{1,0}$ (triangles) and from untreated rats, AF control group (circles).

We have also measured the relative fractional weight of hemoglobin derivatives, namely of: desoxy-, oxy-, carboxy-, sulf- and meth-forms of hemoglobin in hemolysate as a function of the duration of ethanol intoxication of white rats and their posterity.

Fractional weight of hemoglobin forms in hemolisate determined from their light absorption. Even slight deviations from the normal level of hemoglobin derivatives have detrimental effects to the tissues. Hemoglobin derivatives except the oxy-form do not permit the transfer of oxygen. Light absorption of whole blood hemolysate results from the superposition of the light absorption by five composition components, derivatives of hemoglobin, namely by oxy-, desoxy-, carboxy-, sulf- and meth-(MetHb) hemoglobin. Each of these five components when dissolved in water as a single solute exhibits its own absorption band. In hemolysate these components are mixed and one can express the resulting light absorption spectrum $A(\lambda)$ as a sum of absorptions of single component multiplied by their concentration in the hemolisate mixture:

$$A(\lambda) = \sum_{i=1}^{5} c_i A_i(\lambda) , \qquad (2)$$

where c_i is the molar concentration of the components, normalized by their total molar mass such that $\sum_{i=1}^{5} c_i = 1$. In hemolysate the hemoglobin forms can be mutually transformed and consequently their concentrations are changed at the expense of each other. Sensitivity of the spectral test to the blood composition is well illustrated by the fact that a decrease of the amount of oxyhemoglobin leads to visible change in the blood color from bright red to purple-blue. To characterize hemolysate composition, we introduce a parameter called fractional absorbing weight v_i of a given light-absorbing

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component calculated as a ratio

$$v_i = \frac{A_i}{\sum_{i=1}^{5} A_i}$$
(3)

of light absorption A_i of hemolisate measured at a given wavelength λ_i to the sum of absorption values measured at these five wavelengths λ_i . By definition we have $\sum_{i=1}^{5} v_i = 1$. The wavelengths λ_i are chosen to achieve the condition $c_i \approx v_i$ for each of five studied hemoglobin derivatives forms. In Table 1 we present our results on measurements of v_i for different groups of rats.

Table 1. Effect of alcohol intoxication on fractional absorbing weight v_i (%) of hemoglobin derivatives.

Grou	Num-	Hemoglobin derivatives				
р	ber of	desoxy-Hb	oxy-Hb	carboxy-Hb	sulf-Hb	Met-Hb
	rats	-	-	-		
AF	6	0.01±0.005	93.24±0.2.47	2.06±1.12	3.22 ± 3.03	1.47 ± 1.75
$A_{1,0}$	3	0.01 ± 0.004	87.14±1,47	2.66 ± 1.05	5.42 ± 0.49	4.76±0.23
$A_{2,0}$	7	$0.01\pm0,004$	88.35±2,70	2.78±0.77	4.20±0.81	4.88±0.89
$A_{4,0}$	4	0.01±0.003	90.87±1,12	3.33±0.35	2.30 ± 0.55	3.46±0.50
$A_{5,0}$	3	0.01±0.005	97.08±0,82	2.10±0.07	0.01 ± 0.01	0.81 ± 0.80
$A_{6,0}$	3	0.025 ± 0.005	92.66±2.92	3.4±0.19	3.28±1.21	1.65 ± 1.40
$A_{6,1}$	6	0.01 ± 0.005	93.15±2.33	4.14±0.22	1.45 ± 1.36	1.06±0.21

According to Table 1 consumption of ethanol during first 4 months leads to the decrease of the oxyhemoglobin and to the increase of methemoglobin amount in the blood of rats. After 5-6-month of alcohol intake, the values of these parameters return to their normal level. Thus, one can conclude that ethanol affects oxidation of hem iron decreasing fraction of oxyhemoglobin in blood.

Groups of rats	Number	Maximum	Total hemolysis,	Maximum
_	of rats	hemolysis, min	min	hemolysis, %
AF, control group	6	5.1+0.1	8.1±0.2	38,52±1,90
$A_{1,0}$	5	5.1+0.2	9.4±0.6	36,05±3.10
$A_{2,0}$	3	5.5±0.5	9.7±0.7	31.94±3.50
$A_{3,0}$	3	5.0±0.1	8.2±1.3	37.30±3.70
$A_{4,0}$	3	4.5 ±0.2	7,3±0.7	39.06±1,30
$A_{5,0}$	3	2.3 ±0.2	6,5±0.7	35.71 ±0.80
$A_{6,0}$	4	4.6±0.3	8.9±0.6	21.37±4.0
$A_{4,1}{}^{l}$	6	3.25±0.10	8.9±0.4	20.90±2.4
$A_{4,1}^{2}$	3	3.40±0.20	7.7±0.5	24.09±3.3
$A_{6,1}^{3}$	6	3.2±0.2	9.00±0.7	18.83±2.2

Table 2. The erythrogram parameters for of different groups of rats.

¹ Posterity of the parents that consumed ethanol during 2 months;

² Posterity of the parents that consumed ethanol during 3 months;

³ Posterity of the parents that consumed ethanol during 2 months.

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Normalization of the fractional weights of hemoglobin derivatives at chronic ethanol intake and even for the next generation of rats is in agreement with the adaptation to the chronic ethanol exposure though the exact mechanism has to be understood yet.

It is known that the alcohol intoxication is accompanied by the activation of freeradical lipid oxygenation [22]. Free-radical lipids are components of erythrocyte membranes. Their state can be tested using the acid erythrogram method [29]. Our data show that the maximum hemolysis of blood for the control group of rats occurs at 5.1 ± 0.1 min (see Table 2 and Fig. 4). The corresponding time parameter for the group of rats that consumed ethanol during 1-3 months is in the same range, while the duration of total hemolysis is somewhat longer. For rats that consumed ethanol during 4-6 months, the time of maximum hemolysis and the time of total hemolysis are significantly lowered (from 4.5 ± 0.2 min to 2.3 ± 0.2 min). For first generation of rats that consumed alcohol during 4-6 months maximum hemolysis is at 3.2 ± 0.2 min, while the time of total hemolysis is 8.4-9.8 min.



Fig. 4. Erythrograms of blood for the control group of rats (squares) and for the rats consumed ethanol during 1 month (circles), 4 months (upward triangles), 5 months (downward triangles) and 6 months (rhombuses).

Results presented above show that the chronic ethanol intake leads to the decrease in the erythrocyte life duration and to the increase in the inhomogeneity of their population and, hence, that the alcohol intoxication induces a disturbances in both structural and functional states of erythrocytes, as well as in the oxygen-transportation function of hemoglobin.

2.4. Absorption spectra for hemoglobin solution doped with Cibacron Blue

Dye Cibacron Blue F3G-A was purchased from Fluca. In Fig. 5 we compare absorption spectra of hemoglobin water solutions doped by Cibacron Blue F3G-A, a dye known to bind proteins [30-33]. Strong binding of albumin to Cibacron Blue resin column is one of

the most commonly used methods for albumin removal from hemolysate. In Fig. 5 we represented absorption spectra for the mixtures of hemoglobin extracted from AF and $AI_{I,0}$ groups with dye. The AF and AI hemoglobin-dye samples where prepared in the equal concentration proportions. Measured spectra are presented in terms of the absorption coefficient:

$$k(\lambda) = -\frac{\lambda \ln\left(I/I_0\right)}{4\pi d}.$$
(4)

It is seen from Fig. 5(a) that in the ranges of short and long wavelength the values of k_{AF} and k_{AI} practically coincide. For short wavelength region (400-430nm) the light absorption is mostly due to hemoglobin molecules (the hemoglobin-to-dye ratio of the



Fig. 5. (a) Absorption spectra of hemoglobin solution mixed with Cibacron Blue dye for: Al_{1,0} (open triangles) and AF control (open squares) groups. Fitting curves composed of seven Gauss-shaped peaks (solid triangless for Al_{1,0} and squares for AF groups) are shown by thin lines superimposed on the corresponding experimental data. (b) Absorption spectra for 0.01 wt.%, (full circles) of Cibacron Blue dye solutions in water. Fitting curves with three Gaussian peaks (fitting parameters are given in Table 4) are shown by thin lines. (c) Positions of the constitutive peaks λ_2 and λ_3 . (d) Ratio of the fitting absorption weights a_2/a_3 for Cibacron Blue water solutions for different concentrations.

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molar extinction coefficients is about 50) and, thus, the coincidence of the absorption coefficients k_{AF} and k_{AI} in this spectral region is due to the same number of hemoglobin molecules in both samples, that is agree with the nominally equivalent concentration proportions for the samples, mentioned above. Plots in Fig. 5(a) corresponding to AF and AI samples have three isosbestic points: at 425, 515 and 675nm. At long wavelength the absorption of hemoglobin drops such that in the region of the absorption band of Cibacron blue (550 nm $< \lambda < 675$ nm) the light absorption by dye molecules prevails (the hemoglobin-to-dye ratio of the molar extinction coefficients is about 0.3) and, hence, the coincidence between k_{AF} and k_{AI} at long wavelengths reveals roughly the same number of dye molecules in the AF and AI samples in a accordance with nominally equivalent compositions. Differences between k_{AF} and k_{AI} spectra are observed in the middle part of the studied spectral region, namely: $k_{AF} > k_{AI}$ at $430 \text{ nm} < \lambda < 520 \text{ nm}$, while it is opposite at $520 \text{ nm} < \lambda < 675 \text{ nm}$, where $k_{AF} < k_{AI}$. Characteristic hemoglobin absorption band corresponding to the light absorption by iron centres with the maximum at $\lambda = 556$ nm is not visible in the spectra of both AF and AI samples (compare Fig. 1 and Fig. 5(a)). This latter is an indication that the hemoglobin molecules interact with dye molecules, creating hemoglobin-dye molecular complexes. Indeed, negatively charged Cibacron Blue dye residues can be electrostatically bound to positively charged side groups of hemoglobin, including the iron centres, and shifting their absorption to longer wave lengths and most probably overlapping with the absorption bands due to polyaromatic central cores of the Cibacron dye molecules.

Observation of the sample cuvette with naked eyes shows that the hemoglobin-dye solution is not fully homogeneous, but contains suspended flakes, which in time fall down to the bottom of the cuvette. Presence of these flakes evidences formation of hemoglobin-dye complexes. To assure that the sedimentation of these flakes does not affect measured spectra, the sample was stirred before each experiment; spectral measurements were performed in the direction from shorter to longer wavelengths and then the sample was again stirred and the spectrum was taken in the reverse direction from longer to shorter wavelengths. Coincidence of the spectra taken in two directions excludes influence of the sedimentation from consideration.

Additional precaution to the measurement procedure concerns the property of dyes to adsorb on solid surfaces including glass walls of the measured cuvette. After few days a solid bluish layer covering the cuvette walls can be seen. To avoid this problem all the spectral measurements were performed on freshly prepared samples.

Another evidence for the hemoglobin-dye complexes follows from the comparison of the shapes of absorption bands for Cibacron Blue water solutions and that for their mixtures with hemoglobin. The absorption band for the hemoglobin-dye mixtures (Fig. 5(a)) is about 20nm broader than it is for pure water dye solutions without hemoglobin (Fig. 5(b)). The shapes of the absorption bands in Fig. 5(a) are non-Gaussian and, thus, implying that these bands are composed of at least two constitutive Gaussian bands centred presumably around 615 and 650nm respectively. The absorption maximum for pure water solutions of Cibacron Blue is located roughly at 615nm and a peak at $\lambda = 650$ nm is not visible, while it shows up as a constitutive peak for the dye mixture with hemoglobin. Thus, to characterize quantitatively the difference in the absorption spectra for *AF* and *AI*_{1,0} samples it is worth to make the deconvolution of the spectra into constitutive peaks by fitting both dependences with a function, which is a superposition of Gaussian peaks:

$$k(\lambda) = \sum_{i=1}^{n} \frac{a_i \sqrt{2}}{w_i \sqrt{\pi}} \exp\left\{-2\left(\frac{\lambda - \lambda_i}{w_i}\right)\right\}^2,$$
(5)

where w_i are half-widths of the constitutive peaks centred in the absorption maximum at the wavelength λ_i with absorption weights a_i , a constant proportional to the number of the molecules responsible for the absorption in the given peak. We have started the fitting of the experimental data by Eq.5 with five initial parameters for constitutive Gaussian peaks λ_i , among which three peaks have been chosen at $\lambda_1^0 = 390$ nm, $\lambda_{1a}^0 = 430$ nm, $\lambda_{1b}^0 = 556$ nm corresponding to the characteristic hemoglobin peaks and other two peaks: at $\lambda_2^0 = 615$ nm and $\lambda_3^0 = 650$ nm. Last two peaks, namely λ_2^0 and λ_3^0 are in the range of the absorption band for Cibacron Blue molecules and thus they can be understood as guess positions for the constitutive peaks composing the absorption band of Cibacron Blue in water. The resulted 5 peaks fitting curves roughly superimpose with the experimental data, though the coincidence is not total (we do not show these graphs here). To improve the fitting we introduced 6th peak at λ_{2a}^0 between λ_{1b}^0 and λ_2^0 peaks and then 7th peak at λ_{3a}^0 between λ_2^0 and λ_3^0 peaks. Insertion of these additional peaks can be approved assigning them to the light absorption of hemoglobin-dye molecular complexes. The best fits of the experimental data in the studied spectral region (400-700 nm) for 7 constitutive peaks are shown in Fig. 5(a) by bright lines superimposed on dark symbols plotting experimental data. Fitting results are summarized in Table 3. The fitting curves perfectly coincide with experimental $k(\lambda)$ dependencies. It is worth noticing that the variation of the initial guess values for λ_{2a}^0 and λ_{3a}^0 peaks within the ranges between λ_{1b}^0 and λ_2^0 , λ_2^0 and λ_3^0 peaks does not change the fitting results. It is important to stress again that to get the fitting results not worse than that shown in Fig. 5(a) one needs at least 7 constitutive peaks. Although playing with initial guess values for fitting parameters choosing them incidentally one can come to other slightly different sets of λ_i values for the fitting parameters (in the worse case we find ± 5 nm from those given in Table 3), such a random choice of the initial guess values does not seem to be motivated.

We, thus, are led to use the fitting parameters mentioned above for the interpretation of the origin of the difference between k_{AF} and k_{AI} spectra.

Peak number	Peak number Fitting parameter		$AI_{1,0}$ group
	λ_1 , nm	374.98	395.60
1	a_1	2.28×10 ⁻⁴	1.22×10 ⁻⁴
	w_1	62.05	48.43
	$\lambda_{{\scriptscriptstyle 1}a}$, nm	406.43	404.52
2	a_{1a}	1.24×10 ⁻⁵	2.67×10 ⁻⁵
	W _{1a}	14.40	18.28
	$\lambda_{_{1b}}$, nm	428.68	445.14
3	a_{1b}	3.59×10 ⁻⁴	3.32×10 ⁻⁴
	W _{1b}	157.09	169.71
	λ_2 , nm	599.79	588.05
4	a_2	2.08×10 ⁻⁴	1.86×10^{-4}
	<i>w</i> ₂	104.56	97.39
	λ_{2a} , nm	594.83	593.3888
5	a_{2a}	6.×10 ⁻⁶	1.11×10 ⁻⁵
	w _{2a}	29.06	30.8090
	λ_{3a} nm	643.78	640.6494
6	a _{3a}	4.61×10 ⁻⁵	6.45×10 ⁻⁵
	W _{3a}	50.74	49.96
	λ_3 , nm	646.68	650.27
7	<i>a</i> ₃	4.28×10 ⁻⁴	4.099×10 ⁻⁴
	<i>W</i> ₃	187.93	164.2823

Table 3. Fitting results for absorption spectra of hemoglobin solution mixed with Cibacron Blue dye (Fig. 5(a)).

To understand the physical origin of the constitutive peaks let us remark that watersoluble dyes belong to a wide class of materials called chromonics (for review see [34]. Below we shortly recall physical properties of chromonics that are of interest for the explanation of our results.

Dye molecules as a rule are of a plank-like shape. The main characteristic property of chromonics is the formation of rod-like aggregates, in which dye molecules stack faceto-face onto each other when dissolved in water. The aggregates are poly-disperse in their length (from dimers, trimers, tetramers and so on up to the long aggregates such that at higher concentrations they might form liquid crystal phases). If the dye molecules stack onto each other without in-plane shift such that the long axis of the aggregates is

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perpendicular to the molecular plane, they are called H-aggregates. The aggregates, in which each next molecule within the aggregate is shifted with respect to its neighbours such that the long axis of the aggregate is tilted with respect to the molecular planes, are called J-aggregates. H- and J-aggregates differ by their optical spectral properties. H-aggregation is accompanied by a shift of light absorption maximum towards shorter wavelength (blue shift) with respect to the non-aggregated molecules (monomers), while J-aggregates display red shift. This spectral shift can be as large as from few nanometers to tens of nanometers and therefore can be at work when explaining the position of the absorption band maximum for the system hemoglobin-dye. We did not find in the literature any information concerning the possibility for Cibacron Blue molecules associate into aggregates in water solutions. Nevertheless some estimation can be done basing on the information concerning the aggregation of similar organic polyaromatic dyes. It has been established [35,36] that the dye aggregation is promoted by a high ratio of relative molecular mass (M_R) of the dye ionic residue to the total mass (M_I) of the ionic groups and the aggregation number can be estimated as

$$N_A = A \times C_{dve} + M_R / M_I \,, \tag{6}$$

where A is a constant and C_{dye} is the dye concentration in water. For Cibacron Blue we find $M_R/M_I \approx 2.5$, which is in the range of the values typical for polyaromatic dyes. For example, according to the reference [37] for C.I.Reactive Black dye this value is 2.46 and the A constant is 0.0035 for C_{dye} measured in [mg/L]. Taking this value of the A constant for $C_{dye} = 1000 \text{ mg/L}$ we obtain for Cibacron Blue the aggregation number $N_A \approx 6$. Therefore, the influence of the aggregation of dye molecules on their optical spectral properties can play important role and below we examine it.

Cibacron Blue has the absorption maximum roughly at $\lambda = 615$ nm and hemoglobin absorption maximum is at $\lambda = 556$ nm. Therefore, the observed red shift of the absorption maximum for the system hemoglobin-dye towards longer wavelength (from approximately 615 nm for water dye solutions to approximately 650 nm for hemoglobindye mixtures (Fig. 5(a)) has to be prescribed to the dye-hemoglobin complexes. It was suggested in [38] that the red shift of the absorption band is characteristic for complexation of Cibacron Blue with proteins containing super-secondary structure termed the "dinucleotide fold with a hydrophobic pocket", which the dye molecules occupy in the protein. However our analysis presented above combined with the same Gaussian deconvolution of absorption spectra for pure Cibacron solution without hemoglobin (see below) shows that the apparent red shift of the absorption band is actually due to the redistribution of the absorption weights of the constitutive peaks, rather than due to their shift along the wavelength axis.

We have measured spectra of Cibacron Blue dissolved in water for several different concentrations and performed deconvolution of the absorption spectra into constitutive Gaussian peaks. The shapes of the spectra suggest at least two constitutive peaks: one at short wavelengths below 400 nm and another one roughly at 615 nm. The result is that two peaks do not fit the experimental data. Then we introduce a third constitutive peak and perform fitting with the following guess positions for the constitutive peaks: $\lambda_1^0 = 400 \text{ nm}$, $\lambda_2^0 = 615 \text{ nm}$, $\lambda_3^0 = 650 \text{ nm}$. The best fitting curve (thick solid line in Fig. 5(b)) with the best fitting parameters given in Table 4, well coincide with the experimental data (dots in Fig. 5(b)). The constitutive Gaussian peaks centered at $\lambda_2 = 605 \text{ nm}$ and $\lambda_3 = 649 \text{ nm}$ are plotted by thin lines in Fig.5(b). Second peak at $\lambda_2 = 605 \text{ nm}$ appears to be more intensive than the third one at $\lambda_3 = 649 \text{ nm}$. We have found that positions of the second and third constitutive peaks for different concentrations remain almost the same, though with a weak trend towards longer wavelengths when the dye concentration increases (Fig. 5(c)).

Peak number	Fitting parameter	Cibacron Blue, 0.01%
	λ_1 , nm	151.5
1	a_1	38983669
	w_1	184
	λ_2 , nm	605
2	a_2	1467962
	w_2	110
	$\lambda_{_3}$, nm	649
3	a_3	119393
	<i>W</i> ₃	46

Table 4. Fitting results for absorption spectra of 0.01 wt.% of Cibacron Blue dye solutions in water (Fig. 5(b)).

The second peak is much higher than the third one. The ratio a_2/a_3 is approximately constant in the studied concentration range (Fig. 5(d)) and, therefore, these peaks do not display progressive aggregation (desegregation) when the dye concentration increases (decreases) and do not allow to conclude about the type (*H* or *J*) of aggregation. Similar situation was recently reported in the reference [39]. These results show that the determination of the type of aggregation (*H* or *J*) in chromonics via concentration dependencies of absorption spectra is not always conclusive. To determine the aggregation type one needs at least two solutions, in one of which the dye molecules are dissolved in solvent as *separate molecules* without aggregation, whereas in another one they should be in the *aggregated state*. Often this is a serious difficulty, because the aggregation of chromonics exhibits so-called isodesmic behaviour [40]: there is no critical concentration at which the aggregation takes place; molecules aggregate even in very diluted solutions. Notice that the isodesmic behavior is agreed with empirical equation (6), which implies that the dye molecules aggregate even when the dye

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concentration vanish. Moreover for very diluted solutions the detected adsorption signal drops and might become lower than the spectrophotometer noise. In such a situation determination of the type of aggregation via absorption spectra cannot be performed.

Position of the constitutive peaks for pure Cibacron solutions (Table 4, Fig. 5(b,c)) is close to those for hemoglobin-dye solutions (Table 3, Fig. 5(a)): λ_2 -peak of the absorption spectra of pure dye solutions corresponds to λ_2 - and λ_{2a} - peaks for the hemoglobin-dye solutions, while λ_3 -peak of the dye solution corresponds to λ_3 - and λ_{3a} - peaks of the hemoglobin-dye solutions. On can suppose that due to binding of the dye molecules to hemoglobin λ_2 - and λ_3 - peaks obtained for pure dye solution split into λ_2 -, λ_{2a} - and λ_3 -, λ_{3a} - peaks respectively. Taking into account that $a_{2a} << a_2$ and $a_{3a} << a_3$ let us compare the ratio a_2/a_3 for dye solution $a_2/a_3 \sim 15$, while for dye with hemoglobin $a_2/a_3 \sim 2$. Therefore the apparent red shift of the absorption band after the binding of dye molecules to hemoglobin is a result of significant redistribution of the weights of the absorption peaks: for hemoglobin-dye solution in comparison with λ_3 -peak, while their positions are modified little.

The fact that the λ_3 -peak increases at the expense the λ_2 -peak implies that these peaks are not simply of chemical nature due to the interaction of the dye molecule with the hydrophobic pocket of the hemoglobin molecule as it is suggested in [38,41], but rather have a structural origin. Under structural origin of the peaks here we understand that one of the two peaks λ_2 or λ_3 might correspond to the light absorption of the dye monomers, while another one can correspond to the aggregated dye molecules. In other words we suggest that apparent red shift of the adsorption maximum (the shift is apparent because actually it is due to the redistribution of the absorption weights between the constitutive peaks) results from the influence of the protein molecules on the aggregation of dye molecules. In water solution dye molecules are associated into aggregates and this latter implies a shift of absorption maximum for the solution with aggregates with respect to that for non-aggregated molecules towards shorter or longer wavelengths depending on the type (H- or J-) of aggregation. At least two scenarios can be expected at the binding of dye molecules with the protein molecules: 1) dye molecules can be nipped off from an aggregate and attached to the protein coil one-by-one or 2) the aggregate can be attached to the protein molecule as whole. In other words, binding of dye molecules with protein according to first scenario will be a process inverse to the aggregation, i.e. the dissociation or disaggregating of the dye molecules and should be accompanied by appearance of a new peak shifted with respect to that for the aggregation or to the change of the ratio of their absorption weights. The superposition of the redistributed peaks will manifests in the spectra as the shift of the experimentally measured absorption band along

the wavelength axis. If one can identify the constitutive peaks corresponding to the monomeric and aggregated dye molecules respectively then their relative position along the light wavelength axis will indicate the type of aggregation and the first scenario should show up as the increase of the peak assigned to the monomers accompanied by the decrease of the peak corresponding to the aggregated molecules. If the attaching of the dye aggregates as whole to the protein molecules favours the aggregation then one expects the opposite situation: the decrease of the monomeric absorption peak accompanied by the increase of the peak assigned to the aggregates.

Returning to the analysis of the plots for light absorption in the system hemoglobindye we state that the same position of the constitutive peaks and the decrease of the λ_2 -peak accompanied by the increase of λ_3 -peak in comparison with the dye solution without hemoglobin, indicates that these spectral changes agree with the idea about the influence of protein on the aggregation of the dye molecules. If binding of dye molecules to hemoglobin is accompanied by the desegregation of dye molecules then one has to accept that the λ_2 -peak corresponds to the aggregates, while the λ_3 -peak is due to monomeric dye molecules and, hence, Cibacron Blue molecules in water are aggregated into H-aggregates. Although our opinion (supported by the preliminary spectral absorption data obtained for non-absorbing proteins) is that the binding of dye molecules to proteins splits the dye aggregates, at present we do not have enough data to identify unambiguously the peaks responsible for aggregates and monomers. This latter remains an open question as well as the number of binding sites and the dissociation constant need to be determined. Exchanging the assignment of the λ_2 and λ_3 -peaks to monomers and aggregates will lead to the opposite conclusion, namely that the Cibacron Blue aggregates are of J type. Whether or not but the redistribution of the weights of the constitutive peaks at their almost constant positions after binding dye to hemoglobin can be due to the influence of protein molecules on dye aggregation and, thus, the idea that protein molecules can split dye aggregates into separated molecules through their binding can be useful for the investigations of chromonics to determine the type of aggregation (H or J) of dye molecules. This test supposes to be more conclusive for non-absorbing proteins, which bind dye molecules, because a shift of the absorption maximum for dye solution mixed with protein would indicate the contribution of the disaggregated dye molecules to the total light absorption.

Another important conclusion following from the analysis of Fig. 5 is that hemoglobin extracted from alcoholised rats has better affinity to dye molecules than that for non-alcoholised rats. Indeed, the constitutive peak at $\lambda_{1b} = 428 \text{ nm}$, which is characteristic for pure hemoglobin in water, is present in the spectra of hemoglobin with dye for both *AF* and *AI*_{1,0} groups and this indicates that not all the hemoglobin sites responsible for light absorption at λ_{1b} are occupied by dye molecules. Thus, the fact that the absorption weight value $a_{1b} = 3.59 \times 10^{-4}$ obtained for the *AF* group, is higher than the

corresponding value for the $AI_{1,0}$ group, namely $a_{1b} = 3.32 \times 10^{-4}$ (see Table 3 and Fig. 5), illustrates the conclusion made above according to which hemoglobin molecules extracted from alcoholised rats have better affinity to dye in comparison to the non-alcoholised *AF* group. Affinity of the dye molecules to proteins is of the electrostatic nature [42]. If dye residues are charged opposite to the protein residue, they can be bound to the protein ionic residues. Better affinity implies that the protein ionic residues in $AI_{i,j}$ samples are less densely packed. In other words it means that in the protein molecular fragments are broken and, as a result, dye have an access to additional sites in the protein molecule.

Results presented above suggest that ethanol intoxication modifies the structure of blood protein molecules, in particular hemoglobin. However to clarify whether ethanol itself, its metabolites or oxygen free radicals induce these conformational modifications, additional experiments are needed.

3.Conclusions

Our results on comparative spectroscopic studies of blood components extracted from alcohol and non-alcohol treated rats indicate that the ethanol intoxication induces conformational modifications of blood proteins. We find that blood of alcohol treated rats is enriched by the desoxy-form of hemoglobin compared to untreated control group. It is established that alcohol intake during first four months leads to the decrease of fractional weight of oxyhemoglobin and to the increase of methemoglobin amount in blood. Further alcohol consumption is accompanied by the recovery of the normal level of hemoglobin derivatives at chronic (longer than 5-6 months) ethanol intake and even for the next generation of rats is in agreement with the adaptation to the chronic ethanol exposure though the exact mechanism has to be understood yet.

Conformational modifications of blood proteins induced by ethanol consumption can be visualized in optical spectra mixing blood protein samples with dyes. Better dye affinity of hemoglobin extracted from alcohol treated rats compared to the untreated control group supports the conclusion that chronic ethanol intoxication induces structural pathologies in hemoglobin molecules.

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Анотація. Метою даного дослідження є перевірка придатності методів оптичної спектроскопії на предмет виявлення конформаційних змін гемоглобіну, індукованих вживанням етанолу. Для цього використовувались два методи, які базуються на порівняльних спектральних дослідженнях гемоглобіну, взятого з крові групи лабораторних щурів, які примусово вживали алкоголь і контрольної групи, тварини якої не піддавались алкогольній інтоксикації, а саме: 1) метод дослідження кінетики оксигенації гемоглобіну і 2) метод дослідження спорідненості молекул гемоглобіну до барвника Cibacron Blue. Виявлено, що після чотирьох місяців вживання алкоголю фракційний вміст оксигемоглобіну зменшувався, тоді як вміст метгемоглобіну зростав. Подальше споживання алкоголю супроводжувалось відновленням нормального співвідношення похідних гемоглобіну. Цей факт узгоджується з відомим явищем адаптації до хронічного вживання алкоголю. На основі аналізу спектрів поглинання водного розчину гемоглобіну з барвником Cibacron Blue показано, що спорідненість молекул гемоглобіну до даного барвника є більшою в алкогольно інтоксикованих щурів у порівнянні з тваринами контрольної групи. Результати досліджень обома методами підтверджують те, що структурна патологія молекул гемоглобіну, індукована етанолом і його метаболітами може бути виявленою оптичними спектральними методами.